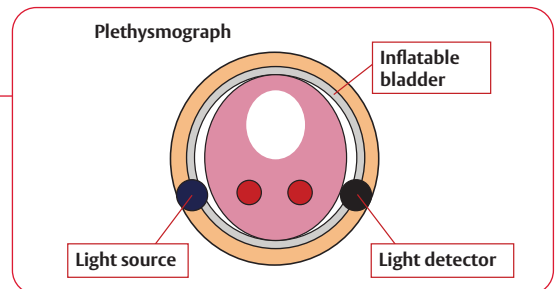


# ClearSight System Technology Overview

## How does it work?

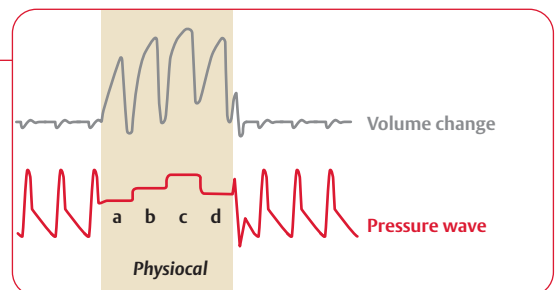
### Volume clamp method

- The essence is to dynamically provide equal pressures on either side of the wall of the artery by clamping the artery to a certain constant volume
- 1000 times each second the cuff pressure is adjusted to keep the diameter of the finger arteries constant
- Continuous recording of the cuff pressure results in a real-time finger pressure waveform<sup>1</sup>



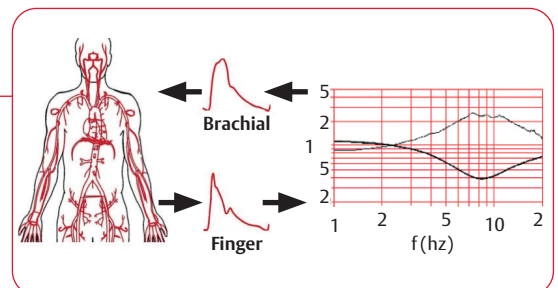
### The Physioal method – Physiological Calibration

- The Physioal method is the real-time expert system that determines the proper arterial 'unloaded' volume, i.e. no pressure gradient across the arterial wall
- Automatic, periodic adjustments are essential to track the unloaded volume clamp setpoint when smooth muscle tone changes (e.g. during vasoconstriction)
- Calibration interval starts at 10 beats, but it increases to every 70 beats as stability increases
- Physioal interval >30 beats is considered reliable<sup>2</sup>



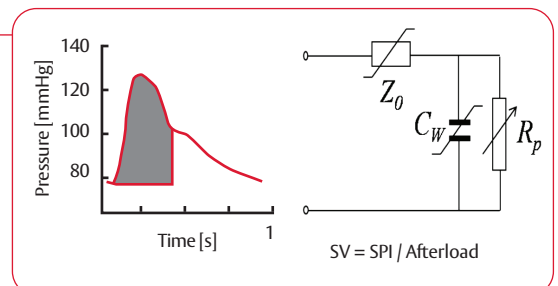
### Brachial pressure reconstruction

- Clinical standard for noninvasive BP is brachial level
- The ClearSight system reconstructs the brachial arterial pressure waveform from the finger arterial pressure waveform
- The reconstruction algorithm is based on a vast clinical database<sup>3</sup>



### Cardiac output calculation

- Stroke volume is calculated by an algorithm based on an improved pulse contour method using:
  - The area under systolic portion of blood pressure curve (Systolic Pressure-time Integral - SPI)
  - A physiological model to calculate afterload individualized by age, gender, height and weight
- Cardiac output results from stroke volume times heart rate and is updated every beat<sup>4</sup>



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Edwards

# Validation of monitoring blood pressure and cardiac output with non-invasive finger cuff technology versus traditional methods

## Blood pressure validation studies

BP can be measured reliably according to AAMI standard, bias <5 and SD < 8 mmHg

Vs. Noninvasive upper arm cuff		Bias ± SD
Akkermans et al. – Hypertension in Pregnancy 2009 <sup>6</sup>	33 pregnant patients	SYS 2.3±6.8 / DIA 0.8±6.3
Eeftinck Schattenkerk et al. – Am J Hypertension 2009 <sup>7</sup>	104 volunteers	SYS 4.3±9.3 / DIA -2.5±8.1
Vs. Invasive radial line		
Martina et al. – Anesthesiology 2012 <sup>8</sup>	50 cardiac surgery patients	MAP 2.2±6.4 mmHg
Fischer et al. – Brit J Anesthesia 2012 <sup>9</sup>	44 cardiac surgery patients	MAP -4.6±6.5 mmHg
Martina et al. – ASAIO J 2010 <sup>10</sup>	18 patients during CPB	MAP -1.3±6.5 mmHg
Vos et al. – Brit J Anesthesia 2014 <sup>11</sup>	112 OR patients	MAP 2.0±9.0 mmHg

## Cardiac output validation studies

Measurement of relative changes in CO performs comparably with invasive measurements

Vs. Noninvasive upper arm cuff		Percentage error
Bubenek-Turconi et al – Anesthesia-Analgia 2013 <sup>12</sup>	28 cardiac surgery patients	38%
Bogert et al – Anaesthesia 2010 <sup>13</sup>	25 post CABG patients	30%
Stover et al – BMC Anesthesiology 2009 <sup>14</sup>	10 severely ill ICU patients	29%
Vs. Transpulmonary thermodilution		
Broch et al – Anaesthesia 2012 <sup>15</sup>	40 cardiac surgery patients	23% / 26%
Hofhuizen et al. – J of Critical Care 2014 <sup>16</sup>	20 post-cardiac patients	38.9%
Vs. Trans-thoracic echo-Doppler		
van der Spoel et al. – J Clin Anesth 2012 <sup>17</sup>	40 ASA 1-2 patients	39%
Vs. Esophageal echo-Doppler		
Chen et al. J Clin Anesth 2012 <sup>18</sup>	25 ASA 1-3 patients	37%

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